

A novel injectable nanotherapeutic platform increasing the bioavailability and antitumor efficacy of Arachidonylcyclopropylamide on an ectopic non-small cell lung cancer xenograft model: a randomized controlled trial

Running title: NanoACPA leads to non-small lung cancer regression in vivo

Ozge Boyacioglu^{1,2}, Cem Varan³, Erem Bilensoy⁴, Zaliha Gamze Aykut⁵, Tuba Recber⁶, Emirhan Nemutlu⁶, Nedret Kilic², Petek Korkusuz^{7,8(*)}

¹ Hacettepe University, Graduate School of Science and Engineering, Department of Bioengineering, 06800, Beytepe, Ankara, Turkey

² Atılım University, Faculty of Medicine, Department of Medical Biochemistry, 06830, Gölbaşı, Ankara, Turkey

³ Hacettepe University, Graduate School of Science and Engineering, Department of Nanotechnology and Nanomedicine, 06800, Beytepe, Ankara, Turkey

⁴ Hacettepe University, Faculty of Pharmacy, Department of Pharmaceutical Technology, 06100, Sıhhiye, Ankara, Turkey

⁵ Bilkent University, Faculty of Science, Department of Molecular Biology and Genetics, 06800, Cankaya, Ankara, Turkey

⁶ Hacettepe University, Faculty of Pharmacy, Department of Analytical Chemistry, 06100, Sıhhiye, Ankara, Turkey

⁷ Hacettepe University, Faculty of Medicine, Department of Histology and Embryology, 06100, Sıhhiye, Ankara, Turkey

⁸ METU MEMS Center, 06530, Ankara, Turkey

Corresponding author

Petek Korkusuz, M.D. Ph.D., Professor of Histology and Embryology

Hacettepe University, Faculty of Medicine, Department of Histology and Embryology, 06100, Sıhhiye, Ankara, Turkey

petek@hacettepe.edu.tr

¹ Özge Boyacıođlu ORCID: 0000-0001-5240-8209

² Cem Varan ORCID: 0000-0002-9391-8691

³ Erem Bilensoy ORCID: 0000-0003-3911-6388

⁴ Zaliha Gamze Aykut ORCID: 0000-0003-2184-8628

⁵ Tuba Reçber ORCID: 0000-0001-8257-7628

⁶ Emirhan Nemutlu ORCID: 0000-0002-7337-6215

⁷ Nedret Kilic ORCID: 0000-0002-5747-9433

⁸ Petek Korkusuz ORCID: 0000-0002-7553-3915

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1 **Abstract**

2 Rapid progressing non-small cell lung adenocarcinoma (NSCLC) decreases treatment success.
3 Cannabinoids emerge as drug candidates for NSCLC due to their anti-tumoral capabilities. We
4 previously reported the controlled release of Arachidonoylcyclopropylamide (ACPA) selectively
5 targeting cannabinoid 1 (CB1) receptor in NSCLC cells in vitro. Hydrophobic polymers like
6 polycaprolactone (PCL) offer prolonged circulation time and slower drug clearance which is
7 suitable for hydrophobic molecules like ACPA. Thus, the extended circulation time with enhanced
8 bioavailability and half-life of nanoparticulate ACPA is crucial for its therapeutic performance in the
9 tumor area. We assumed that a novel high technology-controlled release system increasing the
10 bioavailability of ACPA compared to free ACPA could be transferred to the clinic when validated
11 in vivo. Plasma profile of ACPA and ACPA-loaded PCL-based nanomedicine by LC-MS/MS and
12 complete blood count (CBC) was assessed in wild-type Balb/c mice. Tumor growth in
13 nanomedicine-applied NSCLC-induced athymic nude mice was assessed using bioluminescence
14 imaging (BLI) and caliper measurements, histomorphometry, immunohistochemistry, TUNEL
15 assay, and Western blot on days 7-21. Injectable NanoACPA increased its systemic exposure to
16 tissues 5.5 times and maximum plasma concentration 6 times higher than free ACPA by
17 substantially improving bioavailability. The potent effect of NanoACPA lasted for at least two days
18 on ectopic NSCLC model through Akt/PI3K, Ras/MEK/Erk, and JNK pathways that diminished
19 Ki-67 proliferative and promoted TUNEL apoptotic cell scores on days 7-21. The output reveals
20 that NanoACPA platform could be a chemotherapeutic for NSCLC in the clinic following scale-up
21 GLP/GMP-based phase trials, owing to therapeutic efficacy at a safe low dose window.

22

23 **Keywords:** Non-small cell lung cancer, Arachidonoylcyclopropylamide (ACPA), polycaprolactone
24 (PCL), cannabinoids, nanomedicine, nanoparticle-based drug delivery system

25 1. Introduction

26 Lung cancer is responsible for the majority of cancer-related mortality worldwide due to its high
27 invasive and metastatic features (Lahiri et al., 2023) with crude and age-standardized incidence
28 rates of 28.3 and 23.0 per 100,000 according to a global burden report published in 2023 (Li et
29 al., 2023). More than 85% of cases are defined as non-small cell lung cancer (NSCLC)
30 (Padinharayil et al., 2023). FDA-approved or currently tested targeted agents are known to inhibit
31 PI3K/Akt, Ras/MEK/Erk and JNK pathways through epidermal growth factor (EGF), ROS proto-
32 oncogene 1 (ROS1), anaplastic lymphoma kinase (ALK), mesenchymal-epithelial transition
33 (MET) or rearranged during transfection (RET) receptors but with low success and systemic side-
34 effects complicating the treatment process (Hsu et al., 2023; Liu et al., 2019; Mausey and Halford,
35 2023).

36 Widely distributed endocannabinoid system components within the respiratory epithelia and the
37 immune cells of the stroma act on major immunophysiological functions of the lung (Corrado et
38 al., 2018; Fantauzzi et al., 2020; Gkoumassi et al., 2007; Wiese et al., 2023) and cannabinoid 1
39 (CB1) receptor presents higher expression than that of cannabinoid 2 (CB2) receptor in the
40 parenchyme of the respiratory system (Turcotte et al., 2016). Cannabinoid ligands emerge as
41 drug candidates for NSCLC treatment due to their anti-proliferative, apoptotic, anti-metastatic,
42 and anti-angiogenic capacities (Boyacıoğlu and Korkusuz, 2023). Pan cannabinoid agonists
43 Tetrahydrocannabinol (Δ^9 -THC) (Preet et al., 2008; Sarafian et al., 2008), Cannabidiol (CBD)
44 (Haustein et al., 2014; Milian et al., 2020; Ramer et al., 2012; Ramer et al., 2014; Ramer et al.,
45 2010a; Ramer et al., 2010b; Vidinsky et al., 2012) and WIN55,212-2 (when applied with CB2
46 agonist JWH-015 (Preet et al., 2011) or Met-AEA (Ravi et al., 2014)) at a range between 10^{-8} - 10^{-}
47 4 M dose inhibited proliferation, chemotaxis, migration and/or invasion and promoted apoptosis of
48 NSCLC cells *in vitro*. The *in vivo* validation of the anti-tumoral effect for Δ^9 -THC, CBD, and
49 WIN55,212-2 revealed a limited performance at a high dose range. Two clinical trials revealed
50 the anti-tumoral effects of Δ^9 -THC in two over nine patients (Guzmán et al., 2006) and of
51 Nabiximols (Δ^9 -THC and CBD) (Twelves et al., 2021) in recurrent glioblastoma with serious side
52 effects. Though presenting as the most potent candidate, Δ^9 -THC is the major psychoactive
53 cannabis constituent, can quickly cross the blood-brain-barrier, currently can be used for very

54 restricted indications, and is less likely to be prospective therapeutics for cancer in the clinical
55 practice (Abuhasira et al., 2018; Calapai et al., 2020; Cristino et al., 2020). Our group previously
56 reported a very low real-time antiproliferative and apoptotic dose window (1.39×10^{-12} M) for a
57 synthetic specific CB1 receptor agonist Arachidonylcyclopropylamide (ACPA) and generated a
58 novel ACPA-loaded polycaprolactone (PCL) nanoparticulate delivery system
59 (PCT/TR2020/050618) (Boyacıoğlu et al., 2021; Boyacıoğlu et al., 2022) in conjunction with its
60 metabolic pathway in NSCLC *in vitro* comparing to other epithelial cancers (Endometrial cancer;
61 10^{-6} M (Bilgic et al., 2017), pancreatic cancer; 10^{-4} M (Brandi et al., 2013; Dando et al., 2013;
62 Donadelli et al., 2011)). PCL is a more hydrophobic polymer with a slow degradation rate
63 providing a prolonged circulation time in the bloodstream and thus, gradual release and slower
64 clearance of the encapsulated drug compared to PLA or PLGA (Assani et al., 2022; Sadeghi et
65 al., 2024) which is the best choice for hydrophobic active molecules, such as ACPA. Although,
66 PCL provided a controlled release of ACPA, as a low-soluble cannabinoid with a shorter half-life
67 and poor stability (Boyacıoğlu et al., 2021; Palrasu et al., 2022), an improvement in the plasma
68 profile with a prolonged circulation of the active molecule including enhanced bioavailability and
69 half-life (Elmowafy et al., 2023) is crucial for therapeutic performance at the tumor site (Bhardwaj
70 and Jangde, 2023; Liu et al., 2024; Öztürk et al., 2024).

71 Herein, we hypothesized that the novel ACPA-loaded PCL-based drug delivery platform
72 (NanoACPA), could exhibit superior bioavailability and systemic exposure compared to free
73 ACPA and inhibit tumor growth by decreasing the proliferation rate, promoting the apoptosis of
74 the tumor cells through Akt/PI3K, Ras/MEK/Erk and JNK pathways *in vivo* NSCLC ectopic
75 xenograft nude mouse model by selectively targeting CB1 receptor. First, the plasma profile of
76 ACPA and NanoACPA system and the complete blood count (CBC) parameters of a wild-type
77 Balb/c mouse model were evaluated. The antitumoral effect of the intraperitoneally administered
78 ACPA and NanoACPA system on tumor size was eventually assessed by bioluminescence
79 imaging (BLI) and caliper measurement. Tumor nodules and potential metastatic loci (lung, costal
80 bone, brain, testis, spleen, kidney, and liver) were evaluated by quantitative histomorphometric
81 analysis. Antiproliferative and apoptotic mechanisms of action of the ACPA and NanoACPA

82 nanomedicine on tumor nodules were assessed by Ki-67 immunohistochemical analysis, TUNEL,
83 and Western blot for caspases, PI3K/Akt, Ras/MEK/Erk, and JNK pathways.

84 **2. Materials and methods**

85 **2.1. Study design**

86 An in vivo randomized controlled trial, predetermined by 80% test power and 95% confidence
87 interval (G-Power v3.1), was conducted under ARRIVE guidelines (Voehringer and Nicholson,
88 2020) following ethics approval by the Institutional Animal Care and Use Committee
89 (BILHADYEK) of Bilkent University (24.11.2021/Approval no:2021/15).

90 **2.2. Plasma profile of ACPA and NanoACPA**

91 NanoACPA was prepared and characterized as previously described (Boyacıoğlu et al., 2021).
92 Briefly, NanoACPA formulation was prepared by the nanoprecipitation method using PCL
93 MW:80,000 Da (#440744-250 G, Sigma-Aldrich). A mixture of acetonitrile:ethanol (9:1; v/v),
94 containing 0.1% (w/v) PCL and 0.01% (w/v) ACPA (#91053, Batch no: 0435943-15, Cayman
95 Chemical, C₂₃H₃₇NO, MW: 343.6 g/mol, purity: ≥98%, colorless liquid, 5 mg/100 ul absolute
96 ethanol, solubility in ethanol: 25 mg/ml, organic solvent content: 95%, solid content: 5%), was
97 used to form the organic phase. This phase was then slowly added to ultra-pure water (1:2 v/v)
98 with 0.05% (w/v) Pluronic F68 at room temperature. After stirring the colloidal mixture, the organic
99 solvent was removed and nanoparticle dispersion was obtained (Boyacıoğlu et al., 2021;
100 Boyacıoğlu et al., 2022). As ACPA encapsulation efficiency and 7-day release profile
101 assessments were previously provided (Boyacıoğlu et al., 2021), to observe the long-term
102 physicochemical stability of NanoACPA, *in vitro* characterization by particle size distribution,
103 polydispersity index (PDI) and zeta potential was performed using Zeta Sizer Nano ZS (United
104 Kingdom) (n=3) (Boyacıoğlu et al., 2021) on the day the formulation was prepared and after 3, 5
105 and 7 days of storage at +4°C, since the maximum time interval between two consecutive
106 administrations was 7 days. As a preliminary step, NanoACPA formulation at 0.5 mg/kg dose was
107 applied to wild-type Balb/c mice, however, no peak was identified in the plasma after 60 minutes
108 of i.v. administration by LC-MS/MS (Supplementary Table 1). Thus, ACPA or NanoACPA

109 formulation at 1.0 mg/kg dose, also determined according to previous studies (Ebrahimi-Ghiri et
110 al., 2019; Kumar et al., 2016; Shafaroodi et al., 2004), in a vehicle of 100 μ l of ethanol:PBS (35:65,
111 v/v, EtOH:PBS), was intravenously (i.v.) administered through the tail vein of 6–8-week-old wild
112 type male BALB/c mice (n=6). Blood samples were collected at 5, 30, 60, 120, 240, and 480 min
113 into K₂-EDTA blood collection tubes and centrifuged at 12000 rpm for 15 min at +4°C to obtain
114 plasma. Previously validated liquid chromatography-tandem mass spectrometry (LC-MS/MS)
115 evaluated the amount of ACPA (Boyacıoğlu et al., 2023). Briefly, 50 μ l plasma was spiked with
116 50 μ l acetonitrile containing internal standard anandamide (10 μ g/ml). Following centrifugation at
117 10,000 rpm for 10 min, the supernatant was analyzed. Plasma profile (Dissociation rate constant
118 (k_d), half-life ($t_{1/2}$), volume of distribution (V_d) and clearance (Cl)) and bioavailability (Area under
119 the curve (AUC), maximum plasma concentration (C_{max}) and time to reach the maximum
120 concentration (T_{max})) parameters were calculated by WinNonlin® pharmacokinetic software.

121 **2.3. Complete Blood Count**

122 The hemogram was evaluated in i.v. ACPA (n=6) or NanoACPA platform (n=6)-injected 6–8-
123 week-old wild-type Balb/c mice. Briefly, peripheral venous blood samples collected at t_0 and t_f
124 (480 min after drug application) were transferred into K₂-EDTA tubes and CBC parameters
125 including hemoglobin (HGB), hematocrit (HCT), red blood cell (RBC), mean corpuscular volume
126 (MCV), mean corpuscular hemoglobin (MCH), mean corpuscular hemoglobin concentration
127 (MCHC), red blood cell distribution width-coefficient of variability (RDW-CV), white blood cell
128 (WBC), absolute lymphocyte count (ALC), lymphocyte (LYMPH), absolute monocyte count
129 (AMC), monocyte (MONO), absolute eosinophil count (AEC), eosinophil (EOS), absolute basophil
130 count (ABC), basophil (BASO) and platelet count (PLT) were analyzed by fully automated blood
131 counting device (XN-1000, Sysmex, Turkiye).

132 Peripheral smears of blood samples were stained with the routine Giemsa staining method by
133 Beckman Coulter Unicel DxH smear preparation staining device (DXH 800 SMS). The slides were
134 treated with Giemsa stain and washed with distilled water for 5 min each and evaluated on an
135 automated microscope attached digital camera by image analysis program (Leica DMB6B,
136 DFC7000T, LASV3 Wetzlar, Germany).

137 2.4. Tumor growth assessment of NSCLC xenografts

138 The highest CB1 agonistic antitumoral effect of ACPA and NanoACPA on A549 NSCLC cells in
139 vitro, in our previous study (Boyacıoğlu et al., 2021), constituted the main rationale for the use of
140 this cell line for tumor induction in vivo in this study. 1×10^6 A549-Luc2 (CCL-185-LUC2, ATCC,
141 Virginia, USA) cells, expanded with F12-K medium (Gibco, New York, USA) enhanced by 10%
142 FBS (Capricorn, Germany) and 8 $\mu\text{g/ml}$ blasticidin (Invivogen, France), were injected in 100 μl
143 PBS subcutaneously into the right flank of 6–8-week-old male athymic BALB/c nude mice for
144 tumor induction (Dothager et al., 2009; Preet et al., 2008). When the tumor nodules reached
145 palpable size (average of 100-150 mm^3) (K and Choppala, 2022; Liu et al., 2023) by caliper
146 measurement (day 35, T35), mice were divided into control (0.9% NaCl/2 days, G1), vehicle-
147 treated (EtOH:PBS, 35:65, v/v per 2 days, G2), NanoACPA (1 mg/kg/week, G3, or 1 mg/kg/2
148 days, G4) or ACPA-treated (1 mg/kg/2 days, G5) groups to be injected in 100 μl intraperitoneally
149 (i.p.) for 7, 14 or 21 days ($n=6$, $N=90$). Comparison of vehicle- or drug-treated groups and negative
150 control healthy nude mice ($n=6$, $N=18$) were done for further analyses following sacrifice on
151 days 7 (SET 1), 14 (SET 2), or 21 (SET 3). Evaluation of the nano system-alone on the NSCLC
152 xenograft model was not performed, since the blank PCL nanoparticles have been already tested
153 inert on NSCLC cells by RTCA in our previous work (Boyacıoğlu et al., 2021).

154 BLI for tumor growth assessment was performed under isoflurane anesthesia after i.p. D-luciferin
155 (150 mg/kg) injection on days 0, 14, and 28 of tumor induction and days 7 (day 42), 14 (day 49),
156 and 21 (day 56) of drug administration (Puri et al., 2022). Images were acquired with IVIS
157 Spectrum in vivo Imaging System (PerkinElmer, Massachusetts, USA) and the measurement of
158 light intensity (bioluminescence unit) observed for luciferase-expressing A549 cell-made tumor
159 nodules was presented in terms of total flux radiance as a calibrated measurement based on the
160 photon emission (Lu et al., 2021).

161 Tumor size was also measured with caliper on days 35 (baseline), 42, 49, and/or 56, and tumor
162 volumes were calculated as $\frac{1}{2} \text{length} \times (\text{width})^2$ (Preet et al., 2008; Ravi et al., 2014). After 7, 14,
163 or 21 days of drug application, animals were sacrificed, tumor nodules were excised, and weights

164 were measured by a high-precision scale and quick-frozen in liquid nitrogen for further analyses
165 (Supplementary Fig. 1).

166 **2.5. Histomorphometric analysis**

167 After fixing a small piece of tumor nodules in 10% phosphate-buffered formalin (pH 7.0), they
168 were dehydrated in a graded series of ethanol, cleared with xylol, and embedded in paraffin. 3-5
169 μm -thickened sections, taken by rotary microtome (Leica, Germany), were deparaffinized and
170 stained with Hematoxylin-Eosin. The tumor area was calculated on each section under a light
171 microscope and digital camera attachment (Akkin et al., 2023). Total lung samples were kept in
172 Bouin's fixative at room temperature (RT) for 1 day for macroscopic superficial metastatic
173 nodules. For micrometastasis evaluation, lung, liver, costal bone, kidney, spleen, testicle, and
174 brain tissues were processed for Hematoxylin Eosin staining. Metastatic tumor, inflammation
175 (edema, congestion, cell infiltration), fibrotic and necrosis/epithelial parenchymal disruption
176 (metaplasia, cell damage) areas were evaluated within a range of 0-4; scored as 0 for no
177 inflammation, fibrosis, metastasis or damage in any area, 1 for granulation tissue and
178 inflammatory cell infiltration, fibroblasts, collagen, metastatic and necrotic cell accumulation,
179 blebbing on the apical surfaces of epithelial cells, loss of epithelial cell interface connections and
180 cellular debris in <25% area, 2 for 25-50%, 3 for 50-75% and 4 for 75-100%. The score criterion
181 of the quantitative histomorphometric analysis is summarized (Supplementary Table 2)
182 (Knoblauch and Himmel, 2019).

183 **2.6. Immunohistochemistry**

184 Tumor nodule sections were passed through xylene and alcohols, treated with 0.1 M citrate buffer
185 and heated for antigen retrieval, then treated with 3% hydrogen peroxide and incubated with Ki-
186 67 primary antibody (#ab15580, Abcam, UK) for 1h at RT. Sections were labeled with HRP-
187 conjugated secondary antibody (#ab236466, Abcam, UK) for 2h at RT, dehydrated in graded
188 series of ethanol. The sections were examined under a light microscope and digital camera
189 attachment. Ki-67 positive tumor cells were counted and divided by the total number of cells in
190 the whole tumor area by Image J software (v1.54h) and the percentage was scored as 1 for <15%,
191 2 for 16-45%, 3 for 46%-75%, and 4 for >75% (Wang et al., 2021).

192 2.7. TUNEL assay

193 Tumor nodule sections were evaluated by *ApopTag Peroxidase In Situ Apoptosis Kit* (#S7101,
194 Merck Millipore, Germany) (Bilgic et al., 2017). Briefly, cleared and dehydrated sections were
195 subjected to Proteinase K (#21627, Merck Millipore, Germany) for 15 min at RT. Sections were
196 kept in a 3% hydrogen peroxide, equilibration buffer, TdT solution, and anti-digoxigenin conjugate,
197 respectively. 3,3'-Diaminobenzidine (DAB) for apoptotic cell nuclei staining and methyl green for
198 background staining were performed and evaluated under a light microscope. Quantitative
199 apoptotic cell indices were determined by dividing the number of apoptotic cells in the whole tumor
200 area by the total cell number by Image J software (v1.54h) (Bilgic et al., 2017).

201 2.8. Western blot

202 Phospho-Akt^{S473} (1:2500, #MAB887, R&D, Minnesota, USA), phospho-PI3K^{Y467/Y199} (1:1000,
203 #ab278545, Abcam, UK), phospho-JNK^{T183/Y185} (1:1000, #MAB1205, R&D, Minnesota, USA),
204 pERK1^{T202/Y204}+ pERK2^{T185/Y187} (1:1000, #P00104, Boster Bio, California, USA), total Akt (1:2500,
205 #MAB2055, R&D, Minnesota, USA), PI3K (1:1000, #MAB6777, R&D, Minnesota, USA), JNK
206 (1:2500, #MAB1387, R&D, Minnesota, USA), ERK1+ERK2 (1:10000, #ab184699, Abcam, UK),
207 cyclin D1/D2 (1:2000, #AF4196, R&D, Minnesota, USA), caspase 3 (1:400, #634101, Biolegend,
208 California, USA), caspase 9 (1:500, #E-AB-30760, Elabscience, China) and internal control
209 GAPDH (1:500, #bs-2188R, Bioss, Massachusetts, USA) protein levels in tumor tissues were
210 determined by Western blot as previously done (Kılıç et al., 2022). Following homogenization and
211 centrifugation of 50 mg of tumor tissue, total protein concentration was measured by bicinchoninic
212 acid (BCA) assay (#23227, ThermoScientific, Massachusetts, USA) at 562 nm. After boiling 30
213 µg protein samples with sample buffer for 5 min at 95 °C, all proteins were separated on 8-12%
214 SDS-PAGE (#1658004, Biorad, California, USA) in 1x running buffer and transferred to PVDF
215 membrane with Transfer blot system (#1704150, Biorad, California, USA). After 2h of the blocking
216 step with 5% non-fat milk or BSA/TBS-t, membranes were kept overnight with primary antibodies
217 +4°C on a shaker. After incubation, the membranes were washed with TBS-t, incubated with a
218 secondary antibody for 1h, and washed again with TBS-t. Due to the limited amount of samples
219 to be used for the analysis of many proteins, mild stripping was performed according to the

220 literature (Litovchick, 2020). Enhanced chemiluminescence was performed for the visualization
221 of bands (ChemiDoc Imaging System, #12003153, Biorad, California, USA). Bands were
222 analyzed against GAPDH by Image Lab version 6.0 (Biorad, California, USA).

223 **2.9. Statistical Analysis**

224 Plasma profile data were distributed non-normally by Shapiro-Wilk test, thus all parameters were
225 evaluated by the Mann-Whitney U test (Xu, 2023). Since raw data regarding CBC parameters
226 showed normal distribution by the Shapiro-Wilk test, significance between time points and groups
227 was separately determined by Student's t-test. Raw data of BLI, histomorphometric analysis,
228 TUNEL and Ki-67 labeling, and Western blot were normally distributed by the Shapiro-Wilk test.
229 Multiple comparisons between groups were evaluated by one-way analysis of variance (ANOVA),
230 and pairwise comparisons were evaluated by the post-hoc Duncan test. Spearman's correlation
231 test assessed the correlation between Ki-67 immunostaining–TUNEL and tumor area by
232 histomorphometric analysis–BLI measurements and tumor volume by caliper–BLI
233 measurements. All data were evaluated within the 95% confidence interval (SPSS v25.0). Graphs
234 were drawn with Graphpad Prism 8.

235 **3. Results**

236 ***3.1. Nanoencapsulation improves the bioavailability of ACPA with no WBC but slight RBC*** 237 ***alteration in wild-type mice***

238 NanoACPA showed a mean particle size of 129.4 ± 0.3 nm, PDI of 0.081 ± 0.006 , and zeta
239 potential of -16.11 ± 0.83 mV on the day the formulation. Average nanoparticle size, PDI and
240 zeta potential of NanoACPA were 135.6 ± 0.8 nm, 0.062 ± 0.024 and -20.16 ± 0.38 mV,
241 respectively, on day 3; they were 145.0 ± 3.7 nm, 0.048 ± 0.010 and -21.14 ± 0.73 mV,
242 respectively, on day 5 and 143.2 ± 3.9 nm, 0.065 ± 0.019 and -16.22 ± 0.47 mV on day 7 (Fig 1a,
243 b) indicating that NanoACPA is physicochemically stable when stored at +4 °C for 7 days.

244 NanoACPA ensured a higher and sustainable plasma concentration with a relatively rapid
245 increase and a significantly higher C_{max} , AUC, and $t_{1/2}$ and lower T_{max} , k_d , V_d , and CI from 5 min
246 to 2h compared to the ACPA in wild-type Balb/c mice (Fig. 1c, d). Both ACPA and NanoACPA

247 caused a slight depression in HGB (Fig. 1f) and red blood cell-related counts (RBC, MCH, MCHC,
248 RDW-CV) (Fig. 1g, i-k) excluding the MCV (Fig. 1h) which was also in line with the peripheral
249 blood smear examinations (Fig. 1v-y). The WBC (LYMPH, ALC, MONO, AMC, EOS, AEC, BASO,
250 ABC) (Fig. 1l-t) and PLT (Fig. 1u) counts remained unchanged following NanoACPA injection.
251 WBC parameters, however, presented a suppression that was assisted by a decrease in HCT
252 count (Fig. 1e) following ACPA application at 8h.

253 ***3.2. NanoACPA prominently inhibits NSCLC growth in ectopic nude mouse xenograft*** 254 ***model on days 7-21***

255 Tumor nodules reached a homogenous size by caliper measurement and BLI in all groups on day
256 35 (T35, M0) following s.c. tumor cell injection in all sets (SET 1, 2 & 3) (Fig. 2a-e, 3a-e, 4a-e).
257 All sets presented an acceleration in tumor growth from day 28 (T28) to 42 (T42, M7) excluding
258 the weekly-applied NanoACPA group (Fig. 2f, 3f, 4f) that provided 67% and 48% of tumor growth
259 reduction compared to control and vehicle, respectively. NanoACPA similarly reduced the tumor
260 weight (Fig. 5a-f), however, weekly-applied NanoACPA presented a maximum efficiency in
261 reducing the tumor growth by BLI and by caliper measurement on day 7 (T42, M7) compared to
262 all other groups including every 2-day application (Fig. 2f-g, 3f-g, 4f-g). Weekly-applied
263 NanoACPA diminished the tumor growth by 42% and 65% on average on day 14 (M14) and 21
264 (M21) compared to control, respectively. Every 2-day-applied NanoACPA exhibited superior
265 performance on tumor growth in terms of weight and volume compared to weekly-applied
266 NanoACPA and all the other groups from day 14 (T49, M14) to 21 (T56, M21) in all sets of
267 experiment (Fig. 3f-g, 4f-g, 5) that exhibited 50% and 96% decrease in tumor growth comparing
268 to control, respectively. Free ACPA application provided a decrease in tumor volume by BLI and
269 caliper measurement but not in tumor weight from day 14 to 21 compared to controls (Fig. 3f-g,
270 4f-g, Fig. 5f). Free ACPA exhibited 77% and 11% decrease in tumor growth on days 14 and 21
271 comparing to control, respectively (Fig. 3f-g, 4f-g). A dramatic alteration in tumor volume was
272 observed by every 2 day-applied NanoACPA presenting 48% and 56% reduction on day 14 (Fig.
273 3g) and 78% and 43% reduction on day 21 (Fig. 4g) compared to control and vehicle by calliper
274 measurement. Free ACPA presented 53% (fig. 3g) and 68% (Fig. 4g) decrease in tumor volume

275 on days 14 and 21 compared to control by calliper measurement. Metastatic foci were not noted
276 in the lungs of the drug-applied and control groups from day 7 to 21 (Fig. 5g-l).

277 **3.3. NanoACPA exhibit anti-tumoral efficacy by Akt/PI3K, Ras/MEK/Erk and JNK pathways**

278 NanoACPA ensured poorer infiltrative cell and vessel density patterns within tumor parenchyma
279 when applied weekly or every 2 days compared to all groups from day 7 to 21 by quantitative
280 histomorphometry (Fig. 6a, c, f).

281 NanoACPA presented maximum efficiency in reducing the tumor area and inflammation on day
282 7 when applied weekly compared to all other groups (Fig. 6c, f). NanoACPA groups exhibited
283 similar better performance on tumor area from day 14 to 21 but a superior effect of every 2-day
284 injection on day 21 on inflammation rate compared to controls (Fig. 6c, f). Free ACPA did not
285 change the tumor area and inflammation rate on day 7 but on days 14 and 21 (Fig. 6c, f). Tumor
286 area measurements by histomorphometry (Fig. 6d, $R^2=0.7787$, $p=0.001$) and tumor volume
287 measurements by caliper (Fig. 6e, $R^2=0.8484$, $p=0.001$) presented a significantly strong positive
288 correlation with BLI measurements. Fibrosis (Fig. 6g) and necrosis (Fig. 6h) scores slightly
289 increased in time at variable levels in drug-applied and control groups.

290 Lung (Fig. 6b), costal bone (Supplementary Fig. 2a), brain (Supplementary Fig. 2b), testis
291 (Supplementary Fig. 3a), spleen (Supplementary Fig. 3b), kidney (Supplementary Fig. 4a) and
292 liver (Supplementary Fig. 4b) samples presented a nonspecific mild to moderate stromal vascular
293 congestion and inflammation with mononuclear cell infiltration and mild edema. Fibrotic
294 alterations or necrotic areas were not observed in these organs (Supplementary Table 3). Foreign
295 body reaction or granulomatous focus was furthermore not detected in the lung (Fig. 6b), spleen
296 (Supplementary Fig. 3b), and liver (Supplementary Fig. 4b). NanoACPA (1 mg/kg/week) and free
297 ACPA reduced inflammation in the lungs compared to vehicle or control on day 7 (Fig. 6i). All
298 drug-applied groups decreased the inflammation level in the lungs compared to vehicle-applied
299 and healthy negative control groups on days 7-14; whereas control and vehicle-applied groups
300 had higher inflammation scores than that of negative control on day 21 (Fig. 6i). NanoACPA (1
301 mg/kg/week) and free ACPA caused a higher score of inflammation in the lungs than that of the
302 negative control on day 21 (Fig. 6i). NanoACPA (1 mg/kg/2 days) lowered the inflammation scores

303 in the lungs compared to free ACPA and vehicle on day 21 (Fig. 6i). NSCLC control group
304 presented a significant increase in inflammation scores, whereas negative control group exhibited
305 a significant decrease over time (Fig. 6i).

306 TUNEL (+) apoptotic tumor cells were abundant collectively in the center and scarce in the
307 periphery of the tumor in all control and experimental groups (Fig. 7b) in accordance with the
308 labelling of positive (Fig. 7d) and negative (Fig. 7e) controls, vice versa for Ki-67 (+) proliferative
309 tumor cells (Fig. 7a). All-drug applied groups increased TUNEL scores (Fig. 7b, f) and reduced
310 proliferation rate of tumor cells by Ki-67 labelling (Fig. 7a, c) comparing control and vehicle-
311 applied groups on days 7-21. Free ACPA presented a higher apoptosis rate than that of every 2-
312 day-applied NanoACPA on days 14-21 (Fig. 7f). Every 2-day NanoACPA application caused a
313 sharp decrease in proliferation index over time (Fig. 7c). A strong negative correlation was
314 detected between the apoptotic index by TUNEL and proliferative cell index by Ki-67 labelling
315 (Fig. 7g, $R^2=0.9009$, $p=0.001$).

316 Both weekly- and every 2-day-applied NanoACPA inhibited p-Akt, p-JNK, p-ERK1/2, CycD1/D2
317 and promoted Casp-9 and cleaved Casp-9 expression compared to vehicle and/or control groups
318 on days 7-21 by Western blot (Fig. 7h-i, k-l, n-o). Free ACPA suppressed p-Akt and CycD1/D2
319 protein expression compared to the vehicle-applied group only on day 21 (Fig. 7h-i, n). Every 2-
320 day-applied NanoACPA and free ACPA suppressed p-PI3K and elevated Casp-3 protein
321 expression compared to control on days 7-21 (Fig. 7h, j, m). Weekly-applied NanoACPA reduced
322 p-PI3K on day 7 and elevated Casp-3 expression on day 21 compared to control by Western blot
323 (Fig. 7h, j, m). Free ACPA inhibited p-JNK and induced Casp-9 and cleaved Casp-9 expressions
324 on days 7-21 compared to control and/or vehicle (Fig. 7k, o, Fig. 8).

325 **4. Discussion**

326 In this research, we report the in vivo biodistribution and anti-tumor efficacy performance of a
327 novel nanotherapeutic for NSCLC. We revealed, for the first time, the plasma profile of ACPA and
328 novel PCL-based drug delivery formulation that establishes an improved bioavailability of ACPA
329 with higher peak concentration of plasma, C_{max} , overall exposure AUC and $t_{1/2}$ and lower k_d , V_d
330 and Cl values comparing to free ACPA with a slight depression in RBC and WBC-related counts

331 in a wild-type mouse model directly validating nude mice heterotypic tumor model (Li et al., 2016).
332 All of the WBC counts and the majority of the erythroid cell parameters (MCV, MCH, MCHC,
333 RDW-CV) remaining intact confirmed the biosafety of the new formulation in terms of systemic
334 tolerability. However, the slight decrease in RBC count with no abnormality of other erythroid
335 parameters should be taken into consideration as a potential adverse event in scale-up animal
336 studies. Here, we report that 1.0 mg/kg free ACPA and NanoACPA presented C_{max} and AUC
337 values of 2.443 and 14.173 ng/ml, and 74.918 and 414.982 min.ng/ml, respectively, at 8 h. The
338 systemic exposure expressed as AUC increased 5.5 times and the peak concentration C_{max}
339 increased 6 times in the plasma profile of nanoparticulate ACPA compared to free ACPA, in this
340 study. Two studies assessed the plasma profiles of the potent psychoactive pan cannabinoid
341 agonist Δ^9 -THC (Torrens et al., 2020) and non-psychoactive pan agonist CBD (Xu et al., 2019) in
342 wild-type mice. Δ^9 -THC at 1.6 and 0.5 mg/kg exhibited mean C_{max} and AUC values of 122 and 22
343 ng/ml and 10054 and 2838 min.ng/ml, respectively, when administered to C57BL/6 mice (Torrens
344 et al., 2020). C_{max} and AUC values of ACPA were lower than that of Δ^9 -THC which was
345 significantly improved by nanoencapsulation. Herein, CB1 agonist ACPA at 1 mg/kg presented
346 also a lower C_{max} value than 10 mg/kg i.v.-administered CBD (C_{max} values are 1350 and 48.7
347 ng/ml at 10 min and 8 h, respectively) to ICR mice (Xu et al., 2019) which was substantially
348 enhanced by entrapping ACPA. Δ^9 -THC presented mean C_{max} and AUC values of 198 ng/ml and
349 28763 min.ng/ml, respectively, at 5 mg/kg (Torrens et al., 2020) showing long-lasting anti-
350 depressant-like (Xu et al., 2019) or psychotropic (Cristino et al., 2020) effects when i.v.
351 administered at high doses. The present study established the lowest dose with a potentially
352 adequate yet-to-be-demonstrated antitumor therapeutic efficacy in vivo for the non-psychoactive
353 ACPA and NanoACPA, through CB1 receptor agonism only, in the frame of other cannabinoid
354 therapeutics for NSCLC (Preet et al., 2011; Shafaroodi et al., 2004). The C_{max} , AUC, and half-life
355 of the drug candidate depend on the dose and/or elimination rate of the drug from the body
356 (Hallare and Gerriets, 2024), which requires further plasma profile analysis of ACPA at higher
357 dose levels to compare with other cannabinoids such as CBD. Still, the improved bioavailability
358 of ACPA with a lower dose via a selective CB1 agonism might enable maximizing the clinical
359 benefit by eradicating potential systemic involvement and the side effects of pan agonists (Lazic

360 and Williams, 2020). Herein, the Cl , $t_{1/2}$, and V_d values of ACPA and nanoparticle-bound ACPA
361 were 209.568 and 47.265 ml/min, 36 and 71 min, and 9323.957 and 4866.329 ml, respectively,
362 at 8 h indicating the improvement of bioavailability of ACPA when applied in PCL-based drug
363 delivery formulation. Within this perspective, the successfully developed NanoACPA system
364 improves the tolerability, safety, and efficacy of ACPA in plasma. The V_d and Cl values of 5 mg/kg
365 i.v.-administered Δ^9 -THC to C57BL/6 mice was calculated as 808 ml and 4.4 ml/min, respectively
366 (Torrens et al., 2020). The same research also revealed the plasma half-lives of 5.0, 1.6, and 0.5
367 mg/kg doses of Δ^9 -THC as 109, 108, and 92 min, respectively (Torrens et al., 2020). Intravenously
368 administered CBD at 10 mg/kg exhibited $t_{1/2}$, Cl , and V_d values of 234 min, 1.983 ml/min, and
369 682.5 ml, respectively, in 35 g-weighted ICR mice (Xu et al., 2019). The half-lives of ACPA and
370 NanoACPA system, in our study, were found to be lower than that of CBD and Δ^9 -THC. On the
371 other hand, ACPA and NanoACPA showed higher Cl and V_d compared to those of CBD and Δ^9 -
372 THC. Free ACPA and NanoACPA representing shorter half-life and higher Cl and V_d could be
373 associated with the lower dose application compared to that of CBD or Δ^9 -THC. Furthermore,
374 high V_d observed by ACPA might reveal that the drug leaves the plasma faster followed by
375 passing into the extravascular areas of the body which may require testing higher doses (Mansoor
376 and Mahabadi, 2023). Overall, the superiority of Cl and V_d values of nanoencapsulation
377 maintained the level of ACPA in the blood for a long time in a high, reliable, and permissible dose
378 compared to free ACPA.

379 Herein, we conducted the experiments regarding the evaluation of the plasma profile of Balb/c
380 mice upon i.v. administration of ACPA and NanoACPA but i.p. administration for antitumoral
381 efficacy of the drugs. Due to the rapid absorption of most substances from the peritoneal cavity,
382 it is known that the systemic exposure (AUC and C_{max}) of a substance administered via the i.p.
383 route is more similar to that of the i.v. route (Al Shoyaib et al., 2019). The absorption rate after i.p.
384 administration has a typical rapidity of one-half to one-fourth compared to i.v. administration (Al
385 Shoyaib et al., 2019) which might indicate similarity in overall exposure. Once absorbed from the
386 peritoneal cavity, small molecules like ACPA (343.6 g/mol) are known to follow the absorption
387 pathway to reach the systemic circulation, as the surface area of the membranes transporting the
388 substances into the portal circulation is significantly larger. Another key factor is to consider

389 whether the i.p. route is appropriate for long-term or repeated treatments. Since ACPA and
390 NanoACPA are applied every 2 days within the scope of this research, i.p. administration
391 becomes more reproducible and easier to perform compared to other routes. Moreover, i.v.
392 administration has technical challenges and is not suitable for large-volume administrations when
393 needed. On the other hand, i.p. administration has various advantages including the
394 administration of large volumes, higher absorption rates, and suitability for repeated
395 administrations (Al Shoyaib et al., 2019). Thus, the antitumoral efficacy experiments were
396 conducted by i.p. injecting ACPA and NanoACPA formulations to nude mice models. I.p. injection
397 is a well-established and reliable protocol for antitumoral activity studies in tumor-induced animal
398 models. The physicochemical properties of nanoparticles significantly influence their ability to
399 traverse biological barriers. ACPA-PCL nanoparticles, with a size of approximately 130 nm and a
400 negative surface charge, are considered relatively small. Nanoparticles within the 100-150 nm
401 range have a prolonged circulation time and increased accumulation at the tumor site, as they
402 effectively penetrate biological membranes and enter systemic circulation with rapid absorption
403 upon i.p. administration resulting in higher bioavailability and lower clearance (Chenthamara et
404 al., 2019). Moreover, the i.p. route can allow for prolonged drug release into the peritoneal space,
405 potentially leading to extended therapeutic effect and ensuring systemic distribution. Therefore,
406 we anticipate that our nanoparticles will not encounter significant obstacles in this regard as our
407 research group has published several *in vivo* studies with PCL nanoparticle administration
408 through the tail vein. The biodistribution and the fate of the nanoparticles are well established.
409 Additionally, NanoACPA targeted higher CB1 receptor-expressing tumor cells *in vivo nude* mouse
410 model without being captured, since the superior antitumoral efficacy of the drug candidate could
411 be examined. I.p. administration, on the other hand, could elucidate the potential of nanoparticle-
412 bound ACPA in the peritoneum. Nevertheless, an efficient and rapid diffusion through the
413 biological membranes was expected from the nanoparticles.

414 Herein, we report for the first time that every 2-day 1 mg/kg dose-applied ACPA and NanoACPA
415 inhibit NSCLC growth in ectopic nude Balb/c mice xenograft model on days 14-21 without causing
416 systemic toxicity, increased infiltration, necrosis, fibrosis, and metastasis. ACPA and the novel
417 NanoACPA system provided a 50% reduction in tumor weight and 60-80% in tumor volume,

418 induced apoptosis in more than 50% of the tumor cells and inhibited proliferation in less than 50%
419 of the tumor cells through caspase, PI3K/Akt, Ras/MEK/Erk and JNK pathways, thus, ensured an
420 efficacy with a 100% survival rate following the induction of NSCLC model on day 21. A very
421 limited number of studies assessed the efficacy of synthetic cannabinoid ligands Δ^9 -THC,
422 WIN55,212-2, MET-F-AEA, JWH-133 and JWH-015 via CB1 and/or CB2 receptors to act on
423 A549, H460 or ED1 cell-made NSCLC nude mouse models for 21-28 days (Preet et al., 2008;
424 Preet et al., 2011; Ravi et al., 2014; Ravi et al., 2016). Daily peritumoral administration of CB1/2
425 pan agonist Δ^9 -THC ($K_{iCB1R}=5.05-80.3nM$; $K_{iCB2R}=3.13-75.03nM$) at 5 mg/kg (Preet et al., 2008)
426 and CB1/2 agonist WIN55,212-2 ($K_{iCB1R}=62.3nM$; $K_{iCB2R}=3.3nM$) at 0.1 mg/kg (Preet et al., 2011)
427 exhibited a similar antitumoral efficacy by providing a 50% decrease in A549 cell-based tumor
428 weight and volume, prevented 30-60% of tumor cell proliferation in SCID mice by Ki-67 immune
429 labelling with an increased 40-50% of the apoptotic cell index by WIN55,212-2 and inhibition of
430 p-FAK, p-Erk1/2, and p-Akt by Δ^9 -THC compared to control on day 28. Every 3-day-applied
431 anandamide analogue MET-F-AEA (CB1/2 agonist) at 5 mg/kg and fatty-acid amide hydrolase 1
432 (FAAH, AEA-degrading enzyme) inhibitor URB597 at 1 mg/kg reduced 30-40% of H460 cell-
433 based tumor weight and volume by inhibiting p-EGFR, p-Erk, and p-Akt, diminished 60-70% rate
434 in Ki-67 scores compared to control and vehicle and reduced the necrotic area thus biological
435 aggressiveness in the ectopic NSCLC model on day 21 (Ravi et al., 2014). ACPA has been able
436 to exhibit a comparable antitumoral capability by sole CB1 agonism on ectopic NSCLC nude
437 mouse model at 1 mg/kg dose by i.p. injection that ensured systemic efficacy by maintaining
438 sufficient blood C_{max} and AUC levels within 8h when loaded in the nanoparticulate system. In this
439 study, weekly-applied NanoACPA presented a greater reduction in tumor volume of NSCLC nude
440 mice on day 7 compared to every 2-day application, however, every 2-day application exhibited
441 a better performance in reducing tumor growth compared to weekly applied NanoACPA from days
442 14 to 21 which might make a contradiction in dose-response relationship. A possible explanation
443 would be the internalization of G-protein-coupled receptors including CB1 receptors (Fletcher-
444 Jones et al., 2020). Long-term cannabinoid treatment is known to cause desensitization and
445 downregulation of the CB1 receptor corresponding to the removal and internalization of the
446 receptor from the cell membrane followed by trafficking to lysosomes for degradation (Al-Zoubi et

447 al., 2019; Piscura et al., 2023). The frequency of CB1 receptor agonist administration, such as
448 with ACPA, can dynamically influence CB1 receptors altering the endocytotic pattern and rate
449 within the cells by agonist-induced desensitization (Fletcher-Jones et al., 2020). Furthermore,
450 repeated cannabinoid exposure is known to display a reduction in desensitization along with
451 adaptive receptor recovery followed by receptor upregulation (Augustin and Lovinger, 2022;
452 Fletcher-Jones et al., 2020). Δ^9 -THC at a dose of 10 mg/kg downregulated CB1 receptor
453 expression in the brain after three days of administration, however, increased its expression on
454 days 14-21 (Breivogel et al., 1999), reflecting the dose-, agonist- and region-dependent recovery
455 of CB1 receptor downregulation around 3-7 days (Piscura et al., 2023). Similarly, tumor cells
456 treated with NanoACPA weekly might recover their CB1 receptors in the cell membrane within
457 one week, potentially leading to continuous desensitization with each subsequent dose. In
458 contrast, tumor cells treated with NanoACPA every 2 days might develop a gradual adaptation to
459 the drug, allowing the drug to exhibit higher efficacy on tumor cells. Additionally, the curative
460 efficacy of a drug could be increased only at low doses following the reduction in the tolerance of
461 the cells (Ozdemir, 2020) and CB1 receptor-specific ligands could provide the benefit of causing
462 fewer severe side effects even with long-term use (Al-Zoubi et al., 2019). Those compensation
463 mechanisms should be considered in scale-up studies while synthetic cannabinoid ligands are
464 translated into oncology clinics as chemotherapeutic candidates.

465 Daily peritumoral administration of WIN55,212-2 with CB2 antagonist SR144528 presented a
466 slight decrease in the antitumoral efficiency in terms of change in tumor volume and proliferation
467 and apoptosis in A549 cell-made ectopic NSCLC nude mouse model (Preet et al., 2011). Daily
468 peritumoral administration of CB2 agonist JWH-133 ($K_{iCB1R}=677\text{nM}$; $K_{iCB2R}=3.4\text{nM}$) at 1 mg/kg or
469 WIN55,212-2 at 0.1 mg/kg with CB1 antagonist AM281 diminished 40-70% of A549 cell-based
470 tumor weight and volume and 30-50% of tumor cell proliferation in SCID mice by Ki-67 immune
471 labelling on day 28 (Preet et al., 2011). Every 3-day-applied CB2 agonist JWH-015
472 ($K_{iCB1R}=383\text{nM}$; $K_{iCB2R}=13.8\text{nM}$) at 7.5 mg/kg lowered approximately 30% of mouse ED1 lung
473 tumor weight and volume and reduced more than 70% of cancer cell proliferation on day 21 (Ravi
474 et al., 2016). Evaluated together, WIN55,212-2, JWH-133, and JWH-015 exhibit equivalent
475 antitumoral potency when applied at different effective doses related to their different affinity

476 indices. On the other hand, ACPA ($K_{iCB1R}=2.2nM$; $K_{iCB2R}=715nM$) induced a higher and faster
477 antitumoral effect on the similar ectopic mouse model compared to CB2-agonistic cannabinoids
478 that might be attributed partly to its higher affinity to the receptor with lower K_i values but also to
479 the abundance of CB1 receptors on NSCLC cells that would ensure a targeted chemotherapeutic
480 potency. Previously many groups including ours reported a diffuse CB1R labelling, in healthy
481 human bronchial and pulmonary cells (Turcotte et al., 2016) and in 90% of CB1R density of
482 human NSCLC lines (A549, H1299, H358, and H838 NSCLC cells) in correlation with qRT-PCR
483 data presenting 250 times higher mRNA expression comparing to CB2R (Boyacıoğlu et al., 2021).
484 Taken together, CB1 agonistic chemotherapeutics acting on lung epithelial apoptotic pathways in
485 vitro (Boyacıoğlu et al., 2021) have been validated in vivo in this study suggesting new nano
486 strategies to prevent systemic toxicity but maintaining low anticancer potency.

487 We previously generated and in vitro tested a PCL-based targeted drug delivery system for
488 NSCLC with a loading efficiency of 40% and a cumulative release of 63.9% in 7 days (Boyacıoğlu
489 et al., 2021). Herein, NanoACPA improved all plasma profile parameters from 5 min to 2h with no
490 WBC but slight RBC change, thus confirming a sustainable plasma concentration in wild-type
491 mice and a lower infiltrative cell and vessel extent pattern within tumor parenchyme in nude mice.
492 Every 2-day-applied NanoACPA exhibited superior antitumoral performance in terms of weight,
493 area, and volume assisted by a sharp decrease in proliferative index over time compared to
494 weekly applied- and other groups on day 21. Cannabinoid-loaded PCL-based drug delivery
495 systems have been designed and tested for MDA-MB-231 breast cancer (Hernan Perez de la
496 Ossa et al., 2012), U87MG human glioma (Hernán Pérez de la Ossa et al., 2013), and RBL2H3
497 rat basophil (Hernan Perez de la Ossa et al., 2013) cells in vitro. However, no other cannabinoid-
498 loaded PCL chemotherapeutical formulation has been generated and assessed for NSCLC.
499 Biodegradable CBD (Hernan Perez de la Ossa et al., 2012; Hernán Pérez de la Ossa et al., 2013)
500 and Δ^9 -THC (Castor and Purdum, 2014; Hernán Pérez de la Ossa et al., 2013)-loaded
501 nano/microsystems provided 60–100% drug loading capacity and cumulative release profile
502 which is in line with ours (Castor and Purdum, 2014; Hernan Perez de la Ossa et al., 2012). Taken
503 together, NanoACPA has been validated for its low-dose antitumor capacity, bioavailability,
504 biocompatibility, and low/no systemic toxicity within the frame of the animal model.

505 This study validated the in vivo antitumoral efficacy of the novel ACPA-loaded nanoparticular
506 system through Akt/PI3K, Ras/MEK/Erk, and JNK pathways that correlate with our previous in
507 vitro findings on the CB1 agonistic acting mechanism by inhibiting Akt/PI3K, glycolysis, pentose
508 phosphate pathways; amino acid biosynthesis, urea, and TCA cycles pathways on NSCLC. This
509 study further revealed that NanoACPA acts on caspase-mediated antiproliferative and apoptotic
510 pathways including Ras/MEK/Erk within the tumor microenvironment. Late diagnosis and rapid
511 and silent progression of lung cancer constitute the main challenge for the curative treatment of
512 the disease. The FDA-approved targeted molecular treatment choices (Hsu et al., 2023; Liu et
513 al., 2019; Mausey and Halford, 2023) are the unique option for advanced or recurrent NSCLC
514 patients and considered upon the actionable oncogenic mutations including EGF, ROS1, ALK,
515 MET and RET receptors that all act on common effector pathways of Akt/PI3K, Ras/MEK/Erk and
516 JNK. ACPA's autophagy-inducing and proliferation-reducing effects have been reported in human
517 pancreatic (Brandi et al., 2013; Dando et al., 2013; Donadelli et al., 2011) and lung (Boyacıoğlu
518 et al., 2021) cancer cells via Akt/PI3K, Ras/MEK/Erk and JNK pathways. Here we demonstrate
519 for the first time its in vivo performance within the NSCLC microenvironment. In contrast, the
520 common in vitro performance of ACPA on epithelial cancers including endometrium (Bilgic et al.,
521 2017), pancreas (Brandi et al., 2013; Dando et al., 2013; Donadelli et al., 2011), and lung
522 (Boyacıoğlu et al., 2021) propose a potential as a chemotherapeutic with very low IC₅₀. Thus, it
523 is worth improving its bioavailability confirming safety for eventual reduction of potential adverse
524 effects in further clinical trials by generating novel nano molecular formulations (Liu et al., 2025).
525 Nabiximols cannabinoid oromucosal spray acting on recurrent glioblastoma in a phase 1 trial
526 (Twelves et al., 2021) and a synthetic cannabinoid derivative Dexanabinol targeting advanced in
527 cytologically confirmed, metastatic or progressive solid tumors (Juarez et al., 2021) have been
528 published and an ongoing clinical tolerability study through escalation of Δ^9 -THC and CBD on 20
529 child cancer patients (ClinicalTrials.gov ID NCT05754840) further suggest the use of
530 cannabinoid-made mediators as potential cancer therapeutics in epithelial cancers such as
531 NSCLC. On the other hand, Δ^9 -THC-made pan agonistic cannabinoids pose major complications
532 in patients including dizziness, fatigue, nausea, and headache due to their high dose therapeutic
533 window (Twelves et al., 2021) despite their antitumoral efficacy. ACPA and NanoACPA,

534 distinctively, exhibited better antitumoral performance with a very low IC₅₀ besides Δ^9 -THC and
535 CBD, both reported in preclinical and clinical studies, without a systemic adverse effect, which
536 highlights its potential therapeutic benefits over other therapeutic options.

537 All data is limited to in vivo ectopic xenograft model performance at a one-month time interval.
538 The plasma profile and pharmacodynamic modeling, in this study, were successfully achieved,
539 however, the plasma profile and the antitumoral effect of i.p. ACPA and NanoACPA formulation
540 were evaluated by single-dose administration, which might be a limitation of this study and
541 requires dose and time adjustment. Moreover, to improve the plasma profile of free ACPA and
542 NanoACPA, conducting experiments with multiple and relatively high doses and testing the
543 therapeutic index by determining the maximum dose that mice can tolerate is crucial. On the other
544 hand, the analysis of plasma profile parameters of ACPA and NanoACPA system at a dose set,
545 based on the output of our previous study (Boyacıoğlu et al., 2021), also lower compared to
546 previous studies (Torrens et al., 2020; Xu et al., 2019), might contribute to the literature and
547 provided a strong basis for pharmacodynamic modeling of NanoACPA system on NSCLC
548 regression. The ectopic subcutaneous tumor model evaluated the safety, tolerability, and
549 antitumoral efficacy of the drug candidate (Stribbling et al., 2024), NanoACPA, on the NSCLC
550 tumor model. On the other side, further researches including orthotopic and metastatic tumor
551 models are required to evaluate the pharmacokinetics and pharmacodynamics of NanoACPA,
552 since these models better simulate the tumor microenvironment and provide a more
553 comprehensive assessment before translating preclinical outcomes to clinical practice (Stribbling
554 et al., 2024). Finally, herein, we did not perform the specific antitumoral effect of ACPA and
555 NanoACPA system on CB1R-knockout or any pathway inhibitor-administered NSCLC mouse
556 model. However, we previously demonstrated the CB1R-mediated real-time effect of ACPA and
557 NanoACPA in the presence of CB1-specific antagonist AM281 on NSCLC cells in vitro. We also
558 did not consider a group receiving blank PCL nanoparticles alone. Since we have determined the
559 blank PCL nanoparticles as inert on NSCLC cells by real-time proliferation analysis in our previous
560 work (Boyacıoğlu et al., 2021), we designed our in vivo experiment model based on the minimum
561 number to prevent unnecessary animals according to the 3R principle.

562

563 5. Conclusion

564 In conclusion, our group has successfully clarified nanoencapsulation, improved the plasma
565 profile and bioavailability of ACPA, a specific CB1 receptor agonist, and increased its peak plasma
566 concentration without causing systemic toxicity. The novel NanoACPA nanomedicine has been
567 efficacious in inducing tumor regression through Akt/PI3K, Ras/MEK/Erk, and JNK pathways at a
568 low dose within 21 days in the ectopic NSCLC nude mice model. The overall output validates the
569 chemotherapeutic potency of the NanoACPA system being a candidate as an anticancer drug of
570 a combined second or third-line treatment protocol of NSCLC and further suggests a targeted
571 cannabinoid-based chemotherapeutic platform for solid tumors in oncology clinics following scale-
572 up preclinical experiments of GLP-manufactured product and GMP-based phase trials
573 encompassing the pharmacokinetics and pharmacodynamics of NanoACPA in orthotopic and
574 metastatic CB1 receptor-knockout tumor models.

575

576 Abbreviations

577	Δ^9 -THC	Tetrahydrocannabinol
578	ABC	Absolute basophil count
579	ACPA	Arachidonoylcyclopropylamide
580	AEC	Absolute eosinophil count
581	ALC	Absolute lymphocyte count
582	ALK	Anaplastic lymphoma kinase
583	AMC	Absolute monocyte count
584	AMPK	5'-adenosine monophosphate-activated protein kinase
585	AUC	Area under the curve
586	BASO	Basophil
587	BCA	Bicinchoninic acid
588	BLI	Bioluminescence imaging
589	CB1	Cannabinoid 1
590	CB2	Cannabinoid 2

591	CBC	Complete blood count
592	CBD	Cannabidiol
593	Cl	Clearance
594	C _{max}	Maximum plasma concentration
595	DAB	3,3'-Diaminobenzidine
596	EGF	Epidermal growth factor
597	EOS	Eosinophil
598	FAAH	Fatty-acid amide hydrolase 1
599	HCT	Hematocrit
600	HGB	Hemoglobin
601	ICAM-1	Intercellular adhesion molecule 1
602	k _d	Dissociation rate constant
603	LAK	Lymphokine-activated killer
604	LC-MS/MS	Liquid chromatography-tandem mass spectrometry
605	LYMPH	Lymphocyte
606	MCH	Mean corpuscular hemoglobin
607	MCHC	Mean corpuscular hemoglobin concentration
608	MCV	Mean corpuscular volume
609	MET	Mesenchymal-epithelial transition
610	MMP2	Matrix metalloproteinase-2
611	MONO	Monocyte
612	NanoACPA	ACPA-loaded PCL-based drug delivery system
613	NSCLC	Non-small cell lung cancer
614	PAI-1	plasminogen activator inhibitor-1
615	PCL	Polycaprolactone
616	PLT	Platelet
617	RBC	Red blood cell
618	RDW-CV	Red blood cell distribution width-coefficient of variability
619	RET	Rearranged during transfection

620	ROI	Region of interest
621	ROS1	ROS proto-oncogene 1
622	RT	Room temperature
623	$t_{1/2}$	Half-life
624	T_{max}	Time to reach the maximum concentration
625	TIMP-1	Tissue inhibitor of matrix metalloproteinases-1
626	TRPV	Transient receptor potential vanilloid receptor
627	V_d	Volume of distribution
628	WBC	White blood cell

629

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632 analysis, Dr. Elif Karakoç for sharing her knowledge and experience in assessing antitumoral
633 efficacy of ACPA and Prof. Dr. Zeynep Şafak Teksin for making the pharmaceutical analysis
634 system available for use.

635 **Conflict of Interest**

636 Authors declare having no financial relationship with any commercial identity leading to a conflict
637 of interest.

638 **Author Contributions**

639 OB designed and performed the experiments, analyzed and interpreted data and wrote the
640 manuscript. CV and EB contributed to the design and preparation of PCL-based drug delivery
641 system and assisted with the evaluation of plasma profile analysis and writing the manuscript.
642 ZGA assisted with animal studies. EN and TR contributed to the evaluation of the amount of
643 ACPA in the plasma by LC-MS-MS for plasma profile analysis. NK provided feedback and support
644 for Western blot analyses. PK conceived the project, supervised the research and wrote and
645 edited the paper. All authors wrote and reviewed the final version of the manuscript.

646 In figure 1, EN and TR generated the data, CV and EB analyzed the data and prepared panel A-
647 D, whereas OB prepared the tables in figure 1, drew the graphs in figure 1E-U and prepared the
648 panel V-Y with PK. In figure 2-4, OB and ZGA generated the data, OB assembled the figure and
649 prepared the graphs in figure 2F-G, 3F-G and 4F-G under the guidance of PK. OB took the photos
650 in figure 5A-E with the help of ZGA. OB prepared the graph in figure 5F and took the photos and
651 prepared the panel G-L in figure 5 with PK. OB generated the histochemical and
652 immunohistochemical data, drew the graphs and assembled the figures of 6-7 and supplementary
653 figures of 2-4. OB and PK together evaluated the histochemical and immunohistochemical data
654 and labelled the images. OB generated the western blot data with the help of NK, analyzed the
655 data, and prepared the panel H-O in figure 7. OB prepared the illustrations in supplementary
656 figure 1 and figure 8.

657 **Ethics Statement**

658 This study was approved by Institutional Animal Care and Use Committee (BILHADYEK) of
659 Bilkent University (24.11.2021/Approval no:2021/15).

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664 **Availability of data and materials**

665 All data supporting the findings of this study are available within the paper and Supplementary
666 Information. Further information is available from the corresponding author upon reasonable
667 request. No custom code was created within the context of this study.

668 **References**

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898

899 **Figure Legends**

900 **Fig. 1. NanoACPA improves plasma profile properties and bioavailability of ACPA with no**

901 **immune reaction in wild-type mice. A-B,** Bar graphs representing the physicochemical stability

902 of NanoACPA in terms of **(A)** particle size distribution and polydispersity index (PDI) and **(B)** zeta

903 potential on the day the formulation was prepared and after 3, 5 and 7 days of storage at +4 °C.

904 **C-D,** Graphs depicting ACPA concentration vs. time of i.v. administered **(C)** ACPA and **(D)**

905 NanoACPA formulation demonstrating plasma profile data with p values (n=6). Significance

906 between groups was assessed by nonparametric Mann-Whitney U test. **E-U,** Mean±SEM graphs

907 of **(E)** hematocrit (HCT, %), **(F)** hemoglobin (HGB, g/dl), **(G)** red blood cell count (RBC) (M/mm³),

908 **(H)** mean corpuscular volume (MCV, fL), **(I)** mean corpuscular hemoglobin (MCH, pg), **(J)** mean

909 corpuscular hemoglobin concentration (MCHC, g/dl), **(K)** red cell distribution width (RDW-CV, %),

910 **(L)** white blood cell count (WBC, K/mm³), **(M)** lymphocyte index (LYMPH, %), **(N)** absolute

911 lymphocyte count (ALC, K/mm³), **(O)** monocyte index (MONO, %), **(P)** absolute monocyte count

912 (AMC, K/mm³), **(Q)** eosinophil index (EOS, %), **(R)** absolute eosinophil count (AEC, K/mm³), **(S)**

913 basophil index (BASO, %), **(T)** absolute basophil count (ABC, K/mm³) and **(U)** platelet count (PLT,

914 K/mm³) in the blood samples obtained before (t₀) and at 8h (t_{final}) following i.v. administration of

915 ACPA and NanoACPA platform to wild-type Balb/c mice (n=6) were depicted. Significance

916 between time points and groups was separately determined by Student's t-test indicating (*) for

917 p<0.05 comparing to NanoACPA at t₀; (#) for p<0.05 comparing to ACPA at t₀; (**) for p<0.05

918 comparing to t₀ in ACPA-administered mice and (##) for p<0.05 compared to t₀ in NanoACPA-

919 administered mice. **V-Y,** Micrographs of the peripheral smears of blood samples of i.v.

920 administered ACPA **(V-W)** and NanoACPA formulation **(X-Y)** collected before (hour 0) and after

921 (hour 8) administration show the erythrocytes with normal morphology, sparse distribution of

922 lymphocytes, neutrophils, monocytes and platelets.

923 **Fig. 2. Weekly-applied NanoACPA inhibits NSCLC growth on day 7 by BLI and caliper**

924 **measurements. A-E,** Representative images of BLI assessed between days 0 (T0) and 42 (T42,

925 M7) of **(A)** 0.9% NaCl (control, G1 from M0 to M7), **(B)** EtOH:PBS (vehicle, G2 from M0 to M7),

926 (C) NanoACPA (1 mg/kg/week from M0 to M7), (D) NanoACPA (1 mg/kg/2 days from M0 to M7)
927 or (E) free ACPA (1 mg/kg/2 days from M0 to M7)-administered A549-luc2-injected nude Balb/c
928 mice. (F) Quantification of bioluminescent intensity (10^8 photons/sec) of ROI (region of interest)
929 vs. time (n=6). Note the differences in radiance values per group and time point in each scale. (*),
930 (#) and (‡): p<0.05 for significance between NanoACPA (1mg/kg/week) and control, vehicle or
931 free ACPA, respectively; (‡‡‡): p<0.05 for significance between NanoACPA (1mg/kg/2 days) and
932 free ACPA by one-way analysis of variance (ANOVA) and post-hoc Duncan's test. (G) Curve
933 indicates the tumor growth measured between the baseline (T28), where the tumor volume
934 reaches an average of 100-150 mm³, and day 7 (T42, M7) of drug application (n=6). (**), (##), (‡)
935 and (‡‡‡): p<0.05 for significance between ACPA (1mg/kg/2 days) and control, vehicle,
936 NanoACPA (1 mg/kg/week) or NanoACPA (1mg/kg/2 days), respectively, by one-way analysis of
937 variance (ANOVA) and post-hoc Duncan's test. (T: Tumor injection; M: Medicine administration;
938 G: Group)

939 **Fig. 3. Repeated NanoACPA dosing inhibits NSCLC growth on day 14 by BLI and caliper**
940 **measurements. A-E**, Representative of BLI assessed between days 0 (T0) and 49 (T49, M14)
941 of (A) 0.9% NaCl (control, G1 from M0 to M14), (B) EtOH:PBS (vehicle, G2 from M0 to M14), (C)
942 NanoACPA (1 mg/kg/week from M0 to M14), (D) NanoACPA (1 mg/kg/2 days from M0 to M14)
943 or (E) free ACPA (1 mg/kg/2 days from M0 to M14)-administered A549-luc2-injected nude Balb/c
944 mice. (F) Quantification of bioluminescent intensity (10^8 photons/sec) of ROI (region of interest)
945 vs. time (n=6). Note the differences in radiance values per group and time point in each scale. (#)
946 and (‡): p<0.05 for significance between NanoACPA (1mg/kg/week) and vehicle or free ACPA,
947 respectively; (‡‡‡): p<0.05 for significance between NanoACPA (1mg/kg/2 days) and free ACPA
948 by one-way analysis of variance (ANOVA) and post-hoc Duncan's test. (G) Curve denotes the
949 tumor growth measured between the baseline (T28), where the tumor volume reaches average
950 of 100-150 mm³, and day 14 (T49, M14) of drug therapy (n=6). (**), (##): p<0.05 for
951 significance between ACPA (1mg/kg/2 days) and control or vehicle, respectively; (***) and (####):
952 p<0.05 for significance between NanoACPA (1mg/kg/2 days) and control or vehicle, respectively,
953 by one-way analysis of variance (ANOVA) and post-hoc Duncan's test. (T: Tumor injection; M:
954 Medicine administration; G: Group)

955 **Fig. 4. High dosage frequency of NanoACPA preserves the reduction of NSCLC on day 21.**
956 **A-E**, Representative of BLI assessed between days 0 (T0) and 56 (T56, M21) of **(A)** 0.9% NaCl
957 (control, G1 from M0 to M21), **(B)** EtOH:PBS (vehicle, G2 from M0 to M21), **(C)** NanoACPA (1
958 mg/kg/week from M0 to M21), **(D)** NanoACPA (1 mg/kg/2 days from M0 to M21) or **(E)** free ACPA
959 (1 mg/kg/2 days from M0 to M21)-administered A549-luc2-injected nude Balb/c mice. **(F)**
960 Quantification of bioluminescent intensity (10^8 photons/sec) of ROI (region of interest) vs. time
961 (n=6). Note the differences in radiance values per group and time point in each scale. (*), (#) and
962 (‡): $p < 0.05$ for significance between NanoACPA (1mg/kg/week) and control, vehicle or free
963 ACPA, respectively; (**) and (##): $p < 0.05$ for significance between ACPA (1mg/kg/2 days) and
964 control or vehicle, respectively; (***) and (###): $p < 0.05$ for significance between NanoACPA
965 (1mg/kg/2 days) and control or vehicle, respectively by one-way analysis of variance (ANOVA)
966 and post-hoc Duncan's test. **(G)** Curve represents the tumor growth measured between the
967 baseline (T28) and day 21 (T56, M21) of drug therapy (n=6). (*), (‡) and (##): $p < 0.05$ for
968 significance between NanoACPA (1mg/kg/week) and control, free ACPA or NanoACPA
969 (1mg/kg/2 days), respectively; (**) and (##): $p < 0.05$ for significance between ACPA (1mg/kg/2
970 days) and control or vehicle, respectively; (***) and (###): $p < 0.05$ for significance between
971 NanoACPA (1mg/kg/2 days) and control or vehicle, respectively, by one-way analysis of variance
972 (ANOVA) and post-hoc Duncan's test. (T: Tumor injection; M: Medicine administration; G: Group)

973 **Fig. 5. Every 2-day-applied NanoACPA exhibits superior performance on tumor weight**
974 **without metastatic foci in the lungs. A-E**, Following sacrifice, tumor nodules of **(A)** control,
975 **(B)** vehicle (EtOH:PBS, 35%, v/v), **(C)** weekly-applied NanoACPA, **(D)** every 2-day-applied
976 NanoACPA, and **(E)** every 2-day-applied free ACPA groups were photographed. **F**, Bar graphs
977 represent the tumor weights (g) of each group after 21 days of treatment. **G-L**, Macro metastasis
978 analysis demonstrated that no visible metastatic areas were noted total lung tissues of **(G)** control,
979 **(H)** vehicle, **(I)** negative control, **(J)** weekly-applied NanoACPA and **(K)** every 2-day-applied
980 NanoACPA groups. (*), (#) and (‡): $p < 0.05$ for significance between NanoACPA (1 mg/kg/week)
981 and control, vehicle or free ACPA respectively; (###) and (##): $p < 0.05$ for significance between
982 NanoACPA (1 mg/kg/2 days) and vehicle or free ACPA, respectively, by one-way analysis of
983 variance (ANOVA) and post-hoc Duncan's test.

984 **Fig. 6. Every 2-day-applied NanoACPA presents maximum efficiency on reducing tumor**
985 **area and inflammation on day 21. (A)** Tile scan micrographs of the tumor nodules in the control,
986 vehicle, weekly-applied NanoACPA, every 2-day applied NanoACPA and free ACPA groups
987 exhibit infiltrative cells, vessels and glandular structures. 40x. N: Necrosis, Arrow: Collagen fibrils.
988 **(B)** Note mild to moderate vascular congestion and mononuclear cell infiltration in lung sections.
989 100x. HE: Hematoxylin-Eosin. (*): Infiltration, C: Congestion. **(C)** Tumor area (μm^2) was higher in
990 the control and vehicle than that of drug-applied groups by quantitative histomorphometry (n=6).
991 **D-E**, Correlation graphs of tumor volume measurements by BLI and **(D)** tumor area
992 measurements by histomorphometry ($R^2=0.7787$, $p=0.001$) or **(E)** tumor volume measurements
993 by calliper ($R^2=0.8484$, $p=0.001$) are shown. Spearman's correlation test. **F-I**, Bar graphs
994 represent the histomorphometric analysis for **(F)** inflammation, **(G)** fibrosis and **(H)** necrosis
995 scores of tumor nodules and **(I)** inflammation scores of lung samples (n=6). (*) and (#): $p<0.05$
996 for significance between groups and time points, respectively, by one-way analysis of variance
997 (ANOVA) and post-hoc Duncan's test.

998 **Fig. 7. All drugs diminish tumor cell proliferation and enhance apoptosis through Akt/PI3K,**
999 **Ras/MEK/Erk and JNK inhibition. A-B**, Micrographs denote the tumor nodules on days 7-21
1000 following drug application by **(A)** Ki-67 and **(B)** TUNEL indirect immunoperoxidase labelling. **(C)**
1001 Bar graph standing for the scores regarding Ki-67-labeled NSCLC cells. Chromogen: DAB,
1002 Nucleus stain: Hematoxylin. 400x (n=6). **(D)** Positive and **(E)** negative control groups by TUNEL
1003 indirect immunoperoxidase labelling. **(F)** Bar graph standing for the scores regarding TUNEL-
1004 labeled NSCLC cells. Chromogen: DAB, Nucleus stain: Hematoxylin. 400x. (n=6) (*) and (#):
1005 $p<0.05$ for significance between groups and time points, respectively, by one-way analysis of
1006 variance (ANOVA) and post-hoc Duncan's test. **(G)** Correlation graph demonstrates the relation
1007 between the apoptotic cell index by TUNEL and proliferative cell index by Ki-67 labelling
1008 ($R^2=0.9009$, $p=0.001$). Spearman's correlation test. **(H)** Western blot analysis indicates the bands
1009 for p-Akt (S473), p-PI3K (Y467/Y199), p-JNK (T183/Y185), pERK1 (T202/Y204) + pERK2
1010 (T185/Y187), total Akt, PI3K, JNK, ERK1+ERK2, cyclin D1/D2, caspase 3, caspase 9 and internal
1011 control GAPDH immunolabeling of control and drug-applied groups on days 7-21. **I-R**, Heatmaps
1012 (left or above the bar graphs) and bar graphs demonstrate relative **(I)** p-Akt/Akt, **(J)** p-PI3K/PI3K,

1013 (K) p-JNK/JNK, (L) pERK1+pERK2/ERK1+ERK2, (M) caspase 3, (N) cyclin D1/D2 and (O)
1014 caspase 9 normalized to GAPDH. (n=3) (*) and (#): p<0.05 for significance between groups and
1015 time points, respectively, by one-way analysis of variance (ANOVA) and post-hoc Duncan's test.

1016 **Fig. 8. ACPA and NanoACPA modulate the tumor microenvironment through key signalling**
1017 **pathways.** Significant metabolites/proteins of caspase-mediated Akt/PI3K, Ras/MEK/Erk and
1018 JNK pathways affected in NSCLC microenvironment following i.p. applications of every 2-day
1019 ACPA or NanoACPA platform.

1020 **Supplementary Fig. 1. Schematic diagram for in vivo tumor model.** A549-luc2 cells were s.c.
1021 injected to nude Balb/c mice on day 0 (T0). Tumor growth was assessed on days 14 (T14) and
1022 28 (T28) by BLI and mice were treated every 2 days either with 0.9% NaCl (G1), vehicle
1023 (EtOH:PBS) (G2), free ACPA (1 mg/kg) (G5) or NanoACPA (1 mg/kg) (G4) or weekly with
1024 NanoACPA (1 mg/kg) (G3) on day 35 (T35, M0) for 7 (T42, M7, SET 1), 14 (T49, M14, SET 2) or
1025 21 (T56, M21, SET 3) days and whole body scan was performed by BLI and tumor nodules were
1026 measured by calliper every week. Samples were collected on days 7, 14 or 21 including negative
1027 controls (n=6, N=108) for further molecular and microscopic analyses. (T: Tumor injection; M:
1028 Medicine administration; G: Group)

1029 **Supplementary Fig. 2. No brain and costal bone metastasis and inflammation are observed**
1030 **in treated and untreated groups.** Micrographs of control and experimental groups show (A)
1031 costal bone and (B) brain tissue sections on days 7-21 following applications. E: Epiphyseal plate,
1032 Ca: Cartilage. HE: Hematoxylin-Eosin, 100x.

1033 **Supplementary Fig. 3. No testis and spleen metastasis and inflammation are observed in**
1034 **treated and untreated groups.** Micrographs of control and experimental groups display (A) testis
1035 and (B) spleen tissue sections on days 7-21 following applications. Elongated spermatids were
1036 noted in the seminiferous tubules in the testicular samples. "{": Seminiferous tubule, (*): Elonge
1037 spermatids. WP: White pulp. HE: Hematoxylin-Eosin, 100x.

1038 **Supplementary Fig. 4. No kidney and liver metastasis and inflammation are observed in**
1039 **treated and untreated groups.** Micrographs of control and experimental groups display (A)

- 1040 kidney and (B) liver tissue sections on days 7-21 following applications. G: Glomerulus. HE:
1041 Hematoxylin-Eosin, 100x.

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